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ACR–ASNR–SCBT-MR PRACTICE PARAMETER FOR THE PERFORMANCE OF MAGNETIC RESONANCE IMAGING (MRI) OF THE ADULT SPINE

PREAMBLE

This document is an educational tool designed to assist practitioners in providing appropriate radiologic care for patients. Practice Parameters and Technical Standards are not inflexible rules or requirements of practice and are not intended, nor should they be used, to establish a legal standard of care¹. For these reasons and those set forth below, the American College of Radiology and our collaborating medical specialty societies caution against the use of these documents in litigation in which the clinical decisions of a practitioner are called into question.

The ultimate judgment regarding the propriety of any specific procedure or course of action must be made by the practitioner in light of all the circumstances presented. Thus, an approach that differs from the guidance in this document, standing alone, does not necessarily imply that the approach was below the standard of care. To the contrary, a conscientious practitioner may responsibly adopt a course of action different from that set forth in this document when, in the reasonable judgment of the practitioner, such course of action is indicated by the condition of the patient, limitations of available resources, or advances in knowledge or technology subsequent to publication of this document. However, a practitioner who employs an approach substantially different from the guidance in this document is advised to document in the patient record information sufficient to explain the approach taken.

The practice of medicine involves not only the science, but also the art of dealing with the prevention, diagnosis, alleviation, and treatment of disease. The variety and complexity of human conditions make it impossible to always reach the most appropriate diagnosis or to predict with certainty a particular response to treatment. Therefore, it should be recognized that adherence to the guidance in this document will not assure an accurate diagnosis or a successful outcome. All that should be expected is that the practitioner will follow a reasonable course of action based on current knowledge, available resources, and the needs of the patient to deliver effective and safe medical care. The sole purpose of this document is to assist practitioners in achieving this objective.

¹ *Iowa Medical Society and Iowa Society of Anesthesiologists v. Iowa Board of Nursing*, ___ N.W.2d ___ (Iowa 2013) Iowa Supreme Court refuses to find that the *ACR Technical Standard for Management of the Use of Radiation in Fluoroscopic Procedures* (Revised 2008) sets a national standard for who may perform fluoroscopic procedures in light of the standard's stated purpose that ACR standards are educational tools and not intended to establish a legal standard of care. See also, *Stanley v. McCarver*, 63 P.3d 1076 (Ariz. App. 2003) where in a concurring opinion the Court stated that "published standards or guidelines of specialty medical organizations are useful in determining the duty owed or the standard of care applicable in a given situation" even though ACR standards themselves do not establish the standard of care.

I. INTRODUCTION

This practice parameter was revised collaboratively by the American College of Radiology (ACR), the American Society of Neuroradiology (ASNR), and the Society of Computed Body Tomography and Magnetic Resonance (SCBT-MR).

Magnetic resonance imaging (MRI) of the spine is a powerful tool for the evaluation, assessment of severity, and follow-up of diseases of the spine. Spine MRI should be performed only for a valid medical reason. While spinal MRI is one of the most sensitive diagnostic tests for detecting anatomic abnormalities of the spine and adjacent structures, findings may be misleading if not closely correlated with the clinical history, clinical examination, or physiologic tests. Adherence to the following practice parameter will enhance the probability of detecting such abnormalities.

Spine MRI has important attributes that make it valuable in assessing spinal disease. Alternative diagnostic imaging tests include radiography, computed tomography (CT), myelography, and CT myelography. Compared with these other modalities, MRI does not use ionizing radiation. This is particularly advantageous in the lumbar area where gonadal exposure may occur, and in the cervical spine to avoid radiation to the thyroid. Myelography requires an invasive procedure to introduce intrathecal contrast agents. Both the puncture and the contrast agent can produce side effects and rarely significant adverse reactions. MRI allows direct visualization of the spinal cord, nerve roots, and discs, while their location and morphology can only be inferred on plain radiography and less completely evaluated on myelography. Compared to CT, MRI provides better soft tissue contrast and the ability to directly image in the sagittal and coronal planes. It is also the only modality for evaluating the internal structure of the cord.

However, MRI has not completely supplanted CT for spine imaging. For example, CT provides better visualization of cortical bone than MRI, and some patients who have contraindications to MRI will require other modalities, usually CT, for primary evaluation. While not a contraindication to spine MRI, metallic hardware in the area of scanning may in some cases limit the usefulness of MRI. In selected cases, more than one of these modalities will be needed for a complete evaluation.

II. INDICATIONS

Indications for spine MRI include, but are not limited to, the evaluation of:

1. Congenital spine and spinal cord malformations
2. Inflammatory/autoimmune disorders
 - a. Demyelinating disease.
 - i. Multiple sclerosis (MS).
 - ii. Acute disseminated encephalomyelitis (ADEM).
 - iii. Acute inflammatory demyelinating polyradiculopathy (Guillain-Barre syndrome).
 - b. Connective tissue disorders, e.g., systemic lupus erythematosus.
3. Infectious conditions
 - a. Spinal infection, including disk space infection, vertebral osteomyelitis, and epidural abscess.
 - b. Spinal cord infection including abscess.
4. Vascular disorders
 - a. Spinal vascular malformations and/or the cause of occult subarachnoid hemorrhage.
 - b. Spinal cord infarction.
5. Degenerative conditions
 - a. Degenerative disk disease and its sequelae in the lumbar, thoracic, and cervical spine.
 - b. Neurodegenerative disorders such as subacute combined degeneration, spinal muscular atrophy, amyotrophic lateral sclerosis.
6. Trauma
Nature and extent of injury to spinal cord, vertebral column, ligaments, thecal sac, and paraspinal soft tissues following trauma.

7. Neoplastic abnormalities
 - a. Intramedullary tumors.
 - b. Intradural extramedullary masses.
 - c. Intradural leptomeningeal disease.
 - d. Extradural soft tissue and bony neoplasms.
 - e. Treatment fields for radiation therapy.
8. Miscellaneous
 - a. Spinal abnormalities associated with scoliosis.
 - b. Syringohydromyelia (multiple etiologies, including Chiari malformations, trauma, etc.).
 - c. Postoperative fluid collections and soft tissue changes (extradural and intradural).
 - d. Preprocedure assessment for vertebroplasty and kyphoplasty.

III. SAFETY GUIDELINES AND POSSIBLE CONTRAINDICATIONS

See the [ACR Practice Parameter for Performing and Interpreting Magnetic Resonance Imaging \(MRI\)](#), the ACR Manual on Contrast Media [1], and the ACR Guidance Document on MR Safe Practices [2].

Peer-reviewed literature pertaining to MR safety should be reviewed on a regular basis.

IV. QUALIFICATIONS AND RESPONSIBILITIES OF PERSONNEL

See the [ACR Practice Parameter for Performing and Interpreting Magnetic Resonance Imaging \(MRI\)](#).

V. APPLICATIONS OF MAGNETIC RESONANCE IMAGING

A. Neoplasms

Due to its ability to localize disease into various compartments (intramedullary, intradural-extramedullary, extradural) MRI is usually the most useful method for evaluating spinal tumors and has superior contrast resolution. CT also is often indicated for evaluating bone in tumors with osseous involvement. MRI is well suited for delineating an abnormal intraspinal lesion, assessing its extent within and outside the spinal canal, and evaluating involvement of the spinal cord and intracanalicular spinal nerves. The administration of intravenous gadolinium-based paramagnetic contrast agents further improves sensitivity for lesion detection, enhances lesion delineation, and distinguishes solid and cystic components.

In addition to spinal tumor evaluation, MRI provides an accurate assessment of osseous neoplasms involving the vertebral column, both primary and metastatic. It helps not only demonstrate the presence and extent of bony involvement but also shows the presence and location of epidural and paravertebral extension and the degree of spinal cord and neural foraminal compression. Overall, MRI appears to be more sensitive than bone scintigraphy using single photon emission computed tomography (SPECT) for detecting metastatic disease [3-5] but may not be as sensitive for detecting small metastases in the posterior elements [6]. MRI is also more sensitive and specific than 18F-FDG-PET for detecting bone marrow metastases and infiltration of the spine and has a great impact in staging cancer patients [7].

B. Infection

In a patient with suspected spinal infection, MRI demonstrates high sensitivity and specificity compared to radiographs and bone scans [8-10]. It can localize the site(s) of infection (e.g., within the disc space, vertebral bodies, or both), assess the extent of epidural and paravertebral involvement, and determine presence of a frank abscess [8,11]. Intravenous administration of gadolinium-based contrast agents increases the sensitivity, conspicuity, and observer confidence in the diagnosis, especially in early stages, and is considered mandatory for identifying abscess formation and guiding needle biopsies [8,10].

MRI can also diagnose and characterize the presence of infections in other spinal regions such as the facet joints, meninges, and spinal cord. Due to its unique ability to characterize intraparenchymal lesions, it is critical for evaluating potential spinal cord infections or abscesses [8].

C. Idiopathic Spinal Cord Herniation

Idiopathic spinal cord herniation is a rare cause of myelopathy that has been increasingly recognized in the last few years with the improved contrast resolution of newer magnets. While it is rare, it can be diagnosed preoperatively on MRI with resolution of symptoms after surgery, thereby making it essential to be aware of the imaging findings of this condition [12-15]. MRI helps demonstrate the location of the cord herniation through the dural defect, to assess the degree of herniation, and determine if there are any cord signal changes, all of which impact patient management and prognosis [12-15].

D. Degenerative Disc Disease

MR imaging provides a precise representation of the anatomy of the disc, spinal canal, and discovertebral complex, information that will allow accurate diagnosis of degenerative disc disease and influence therapeutic decision making [16]. It is well established as the modality of choice for evaluating degenerative disease of the spine, although in selected patients CT may be an alternative for assessing the lumbar spine [17].

E. Spinal Stenosis

The anatomic assessment provided by MRI allows accurate evaluation of both acquired and developmental spinal stenosis. MRI can assess the morphology of the spinal canal itself, as well as the intervertebral foramina and nerve root canals, to accurately characterize the presence [18-19] as well as type of stenosis [18]. It may also be useful in identifying other causes of spinal stenosis in which the osseous architecture is unremarkable, such as epidural lipomatosis [20].

F. Intramedullary Disease

MR imaging, without and/or with intravenous contrast, is almost unique in its capability to demonstrate the presence and extent of spinal cord disease processes of many different etiologies: demyelinating, neoplastic, degenerative, inflammatory, metabolic, traumatic, ischemic, congenital, etc. No other spinal imaging modality, invasive or noninvasive, reliably allows the detection and, in many cases, the differentiation of intramedullary processes that do not expand the spinal cord.

G. Trauma [2,21-30]

MR imaging is a valuable tool for assessing patients with known vertebral injury. In addition to assessing the fractures themselves, it can aid in evaluating the integrity of ligaments, which may predict spinal stability. It also contributes to imaging the spinal cord for transection, contusion, edema, or hematoma. Cord compression by bone fragments, disc herniation, and epidural or subdural hematomas can also be demonstrated. Serial examination of patients with hemorrhagic contusion within the cord can reveal the onset of post-traumatic progressive myelopathy. Furthermore, refinement of MR angiography (MRA) can provide information about the vertebral arteries. MR imaging is also useful in patients with equivocal findings on CT examinations by searching for evidence of occult injury (edema, ligament injury). Finally, MR imaging can help to predict whether osteoporotic compression fractures are acute or chronic when there are no previous studies for comparison.

H. Iatrogenic Changes of Radiotherapy to the Spine

Radiation therapy has been a mainstay of treatment of neoplastic diseases. Unfortunately, radiation therapy that includes the spine can also result in unintended iatrogenic complications. These complications can occur to both the vertebral column and the underlying spinal cord.

In the vertebral column, the most benign changes are well seen by MRI and initially consist of marrow edema, followed by fatty replacement of the marrow. These changes can occur as soon as a few weeks after the cessation of radiation therapy. More serious complications include radiation osteonecrosis [31-32]. Radiation osteonecrosis is most common after treatment for head and neck tumors, although it can be seen following radiation therapy for other neoplasms as well. Typically, radiation osteonecrosis results in degeneration and collapse of the involved vertebral body. Superimposed osteomyelitis may complicate the clinical scenario. MRI is not only superb in localizing the involved vertebral body but can also suggest a diagnosis through the visualization of vertebral body destruction and fragmentation.

Radiation therapy can also induce complications of radiation myelopathy [33-42]. Acute radiation myelopathy does not produce MR findings. However, in later stages radiation myelopathy typically results in mass effect, swelling, and rim enhancement, followed by atrophy. MRI is particularly suited in making the diagnosis of radiation myelopathy due to its ability to portray the underlying cord lesion, with characteristic ring enhancement, associated with radiation changes in the spinal column, ranging from fatty infiltration to radiation-induced bone infarcts and necrosis.

Radiation therapy can lead to the development of treatment-related tumors several years to several decades later [43]. These include bony neoplasms of the vertebral column, intradural extramedullary tumors such as meningiomas, and gliomas of the cord. Again, MRI can portray the association of the neoplasm with the classic changes of prior radiation in the vertebral column.

I. Vascular Lesions of the Spine

Multiple vascular lesions can affect the spine. There are two general categories, spinal cord ischemia and vascular malformations. MRI is the most sensitive method of verifying the presence of cord ischemia and infarction [44-45]. As in the brain, diffusion weighted imaging is particularly sensitive and diagnostic in the appropriate clinical settings. Conventional MRI, however, can also demonstrate classic findings of cord infarction, with hyperintense signal acutely involving the anterior half to two-thirds of the cord or being centered primarily in the grey matter. In addition, associated vertebral body infarction can be seen [46]. Due to the small size of the multiple collaterals that feed the cord, MR angiography is generally not as useful in this clinical setting.

Vascular malformations are comprised of arteriovenous malformations (AVMs) and cavernous hemangiomas [47-51]. AVMs are classified in the Anson and Spetzler system into four groups. MR imaging is the most successful noninvasive method of assessing the spine for vascular malformations. Multiple findings can be seen, including the presence of frank fistulas, a nidus of serpentine signal voids in AVMs, or posteriorly draining enlarged veins in dural arteriovenous fistulas (AVFs). In addition, MR imaging is also sensitive to secondary changes in the cord, such as venous congestion and gadolinium enhancement. MRA, with or without contrast administration, can also play a role in detecting and characterizing these lesions [46]. It is helpful in depicting pial fistulas and dural AVFs and can be useful in guiding subsequent spinal angiography.

Occult vascular malformations, including cavernous angiomas and partially thrombosed arteriovenous malformations, as in the brain, generally appear as focal lesions containing byproducts of hemoglobin degradation [48]. In the majority of cases, virtually no surrounding edema is present, unless there has been recent bleeding. Using sequences sensitive to local variations in magnetic susceptibility, MR is very sensitive in the detection of suspected cavernous hemangiomas. In addition, the absence of surrounding cord swelling and edema are also well depicted on MR imaging, allowing differentiation from neoplasms.

J. Congenital Lesions

Coil selection and field of view will depend on patient size and the region imaged. A spine coil should be considered while larger patients may be imaged with a cardiac, torso, spine, or body coil. Commercially available combined coil arrays may also be suitable.

Imaging sequences should include T1-weighted and T2-weighted sequences, preferably in two planes. This can be achieved using conventional, fast or turbo spin echo, or gradient echo sequences with slice thickness dependent on the area to be imaged (usually 3 to 5 mm). Fat suppression techniques are also valuable to confirm congenital fatty lesions. Physiologic motion suppression techniques and software may help optimize image quality.

In case of spinal curvature (scoliosis), imaging in the plane of the spine, both sagittal and cross-sectional, should be attempted and may require multiple acquisitions with compound and/or complex angles to cover the areas of concern.

Use of intravenous contrast agents may increase conspicuity of the anatomy and pathology relative to surrounding vascular structures and may help to define avascular areas.

K. Demyelinating Diseases

MR imaging, without and with intravenous contrast, is the examination of choice for the imaging diagnosis and follow up of demyelinating processes affecting the spinal cord. Only MRI can identify the extent of disease and the response to therapy, if any, although lesion burden does not correlate well with clinical status in patients with multiple sclerosis [52]. Advanced imaging techniques, such as diffusion tensor imaging and spectroscopy, may be valuable adjuncts [53-54].

Application of this practice parameter should be in accordance with the [ACR Practice Parameter for Performing and Interpreting Magnetic Resonance Imaging \(MRI\)](#) and the [ACR–SIR Practice Parameter for Sedation/Analgesia](#).

VI. SPECIFICATIONS OF THE EXAMINATION

The supervising physician must have complete understanding of the indications, risks, and benefits of the examination, as well as alternative imaging procedures. The physician must be familiar with potential hazards associated with MRI, including potential adverse reactions to contrast media (potential hazards might include spinal hardware if recently implanted, especially in the case of neoplasia or significant trauma). The physician should be familiar with relevant ancillary studies that the patient may have undergone. The physician performing MRI interpretation must have a clear understanding and knowledge of the anatomy and pathophysiology relevant to the MRI examination.

The written or electronic request for MRI of the adult spine should provide sufficient information to demonstrate the medical necessity of the examination and allow for its proper performance and interpretation.

Documentation that satisfies medical necessity includes 1) signs and symptoms and/or 2) relevant history (including known diagnoses). Additional information regarding the specific reason for the examination or a provisional diagnosis would be helpful and may at times be needed to allow for the proper performance and interpretation of the examination.

The request for the examination must be originated by a physician or other appropriately licensed health care provider. The accompanying clinical information should be provided by a physician or other appropriately licensed health care provider familiar with the patient's clinical problem or question and consistent with the state's scope of practice requirements. (ACR Resolution 35, adopted in 2006)

The supervising physician must also understand the imaging parameters, including pulse sequences and field of view, and their effect on the appearance of the images, including the potential generation of image artifacts. Standard imaging protocols may be established and optimized on a case-by-case basis when necessary. These protocols should be reviewed and updated periodically.

A. Patient Selection

The physician responsible for the examination should supervise patient selection and preparation and be available in person or by phone for consultation. Patients must be screened and interviewed prior to the examination to exclude individuals who may be at risk by exposure to the MR environment.

Certain indications require administration of intravenous (IV) contrast media. IV contrast enhancement should be performed using appropriate injection protocols and in accordance with the institution's policy on IV contrast utilization. (See the [ACR–SPR Practice Parameter for the Use of Intravascular Contrast Media](#).)

Patients suffering from anxiety or claustrophobia may require sedation or additional assistance. Administration of moderate sedation may be needed to achieve a successful examination. If moderate sedation is necessary, refer to the [ACR–SIR Practice Parameter for Sedation/Analgesia](#).

B. Facility Requirements

Appropriate emergency equipment and medications must be immediately available to treat adverse reactions associated with administered medications. The equipment and medications should be monitored for inventory and drug expiration dates on a regular basis. The equipment, medications, and other emergency support must also be appropriate for the range of ages and sizes in the patient population.

C. Examination Technique

1. General principles

Physicians who determine the pulse sequences to be used and interpret spine MR examinations must understand the artifacts associated with and the limitations of the various imaging pulse sequences. MRI of the spine involves the application of various MR pulse sequences that are designed to provide a range of imaging characteristics and capabilities. These include the following:

- a. Variable soft tissue contrast, e.g., T1-weighted, T2-weighted, and T2*(T2 star)-weighted images.
- b. Direct multiplanar display, e.g., sagittal, axial, and coronal images.
- c. Darkening of certain tissues (e.g., fat) or defined regions (e.g., anterior abdomen) of an image by suppression of their MR signal.
- d. Flow (cerebral spinal fluid [CSF] or blood) sensitization or desensitization.

The MR signal that is produced from a region of the spine (cervical, thoracic, and lumbosacral) in response to a particular pulse sequence is often, but not always, detected using dedicated surface coil receivers, commonly in a phased array configuration. Two-dimensional (2D) or three-dimensional (3D) data sets are generated from the received MR signal intensities.

In addition to images with contrast based on intrinsic MR properties of the spinal and paraspinal tissues, some images may be acquired after the intravenous administration of a paramagnetic MR contrast agent (e.g., a chelate of gadolinium). This agent is used to detect regions where the normal vascular circulation has been altered by injury or disease. For example, the use of intravenous paramagnetic contrast is recommended for distinguishing recurrent or residual disc material from scar tissue in patients who have undergone prior spinal surgery.

2. Pulse sequences

The choice of MR pulse sequences is guided by the clinical history and physical examination and is based on the indications for the study (see section III, Indications). Certain sequences are commonly used in MR imaging of the spine. These include:

- a. Two-dimensional T1-weighted sagittal imaging.
- b. Two-dimensional T2-weighted or T2*-weighted sagittal imaging.
- c. Two-dimensional T1-weighted axial imaging.

d. Two-dimensional T2-weighted or T2*-weighted axial imaging.

Three-dimensional implementations of these images are progressively used and may replace the two-dimensional methods.

The pulse sequences described above may be modified to suppress the MR signal from lipid-containing regions, producing images in which fat is dark. T1-weighted images with fat saturation are primarily acquired as part of studies that include the intravenous administration of a paramagnetic contrast agent. Short tau inversion recovery (STIR) methods often are performed to increase conspicuity of osseous and ligamentous lesions. For the purpose of comparison, images with fat suppression are sometimes acquired before and after administration of the contrast agent. Alternate approaches to fat suppression, such as three-point Dixon methods, may be used instead.

Low-flip-angle sequences with intermediate to long TE values produce T2*-weighted tissue contrast. This has similarities to T2-weighted contrast but is usually more sensitive to local magnetic field inhomogeneities (e.g., greater signal loss at interfaces between bone and CSF or between bone and soft tissue) and less sensitive to CSF flow-induced artifacts (e.g., signal voids due to brisk or pulsatile CSF flow).

Another commonly used modification is the set of MR pulses that produce spatial saturation zones anterior, inferior, and/or superior to the spinal region of interest. This suppresses signal from these regions, so that motion outside the intended field of view (e.g., breathing, blood flow) produces less conspicuous phase encoding artifacts and less degradation of the spinal images.

Due to anatomical and physiological differences in three major spinal regions, radiologists are more likely to use certain sequences in one region than in another. In the cervical and thoracic spine, CSF flow is normally more dynamic than in the lumbosacral spine, and T2*-weighted axial and sagittal images are often acquired because these are less apt to have CSF flow-related artifacts than are T2-weighted fast-spin-echo images. In the cervical spine, where the neural foramina are generally smaller than those in the thoracolumbar region, gradient-echo or fast-spin-echo pulse sequence data may be acquired in three dimensions in order to provide higher spatial resolution and postprocessed multiplanar display of the foramina. In the lumbosacral spine, T1-weighted axial images benefit from the tissue contrast between abundant high-signal-intensity epidural fat juxtaposed to low-signal-intensity CSF and intermediate signal intensity epidural lesions (e.g., disc herniation).

Minimum recommended pulse sequences for evaluating the spine for pain, radiculopathy, or suspected stenosis may include:

- a. Cervical/thoracic spine
 - Sagittal T1-weighted
 - Sagittal T2-weighted or T2*-weighted
 - Axial T2-weighted or T2*-weighted
- b. Lumbar spine
 - Sagittal T1-weighted
 - Sagittal T2-weighted or T2*-weighted
 - Axial T1-weighted and/or T2-weighted

In postoperative cases for differentiating scar from disk, postcontrast sagittal and axial T1-weighted series with or without fat suppression are useful. When evaluating spinal bone marrow for tumor, sagittal T1-weighted sequences, as well as short TI inversion recovery (STIR) sequences, fat-suppressed T2-weighted fast-spin-echo sequences, or other fat suppressed acquisitions are recommended. In addition, a contrast-enhanced or a fat suppressed contrast enhanced study can evaluate extraosseous extension of a neoplastic process. When evaluating soft tissues after trauma or surgery, STIR or other T2-weighted fat-suppressed fast-spin-echo sequences are recommended.

3. Slice thickness

The following are recommended maximum slice thicknesses for performing the typical spine examinations:²

<u>Sequence</u>	<u>Slice Thickness</u>	<u>Gap</u>
Cervical spine - sagittal	≤ 3 mm	≤ 1 mm
Cervical spine - axial	≤ 3 mm	≤ 1 mm
Thoracic spine – sagittal	≤ 4 mm	≤ 1 mm
Thoracic spine – axial	≤ 4 mm	≤ 1 mm
Lumbar spine – sagittal	≤ 4 mm	≤ 1 mm
Lumbar spine – axial	≤ 4 mm	≤ 1 mm

4. Area of coverage

The imaging protocol should be designed to cover the area of clinical interest. Because the clinical situation is a crucial determinant of treatment, the following are general recommendations and not strict criteria.

For pain, radiculopathy, suspected stenosis, or other degenerative conditions:

Cervical spine: Sagittal and axial images should include from the atlanto-occipital joints through at least the C7 to T1 intervertebral disc.

Thoracic spine: Sagittal and axial images should include the area of clinical interest. If the entire thoracic spine is to be studied, C7 to L1 should be imaged in the sagittal plane, with axial images obtained as warranted. For thoracic imaging, visualization of the craniocervical junction is useful for accurate localization of thoracic levels and pathology.

Lumbar spine: The entire lumbar spine should be studied on the sagittal images (T12 to S1), and axial images should be obtained through at least the lowest three lumbar discs (L3/4, L4/5, and L5/S1). Axial images through other discs can be obtained as needed. Sagittal imaging should include the entire lumbar spine, including parasagittal imaging of all of the neural foramina on both sides. Imaging should permit counting spinal levels if necessary. Tailored examinations may be appropriate for follow-up of known pathology.

For tumor and infection, sagittal and axial images should include the area of clinical interest. If other imaging modalities or the clinical evaluation narrow the levels of suspected abnormalities, then at times it may be appropriate to limit MRI to these areas of interest. If MRI is to be used as the only diagnostic imaging modality for clinically occult disease, screening of the entire spine may be indicated.

²Thicker slices may be acceptable when the goal of the examination is primarily to survey most or the entire spine.

5. Other techniques

a. Parallel imaging [55-61]

Parallel imaging (PI) uses the spatial sensitivity information from phased-array radiofrequency (RF) coils to reduce the number of phase-encoding steps and therefore shortens the time of image acquisition. These time savings imply a loss of signal-to-noise ratios, but without compromising image contrast or spatial resolution. The coil sensitivity information is obtained by performing a prescan calibration or by obtaining additional lines of k-space with each sequence as “auto calibration.” Numerous image reconstruction algorithms have been developed including space domain based techniques (SENSE), k-space regenerative techniques (SMASH, generalized SMASH and GRAPPA) and other hybrid techniques (SPACE-RIP). The maximum reduction in imaging time, reflected in parallel imaging acceleration factor, is 2 to 3 in each phase-encoding direction. The limitation of the accelerating factor is due to increased noise associated with both reduced temporal averaging and the reconstruction process. The reduction in signal-to-noise ratio associated with higher parallel imaging factors can be counterbalanced by the increased signal-to-noise ratio at higher fields. When imaging a small field of view, the sensitivity maps may be used to reduce wraparound artifact if the images are acquired without reduced k-space sampling.

Parallel imaging is applicable to all pulse sequences and complementary to other existing acceleration methods. In spine imaging, pulse sequences with high contrast and spatial resolution can be combined with PI and allow evaluation of disc pathology, cord and nerve root impingement, and neural foraminal patency. In 3D imaging, the phase-encoding steps can be reduced in 2 directions, for a maximum parallel imaging factor of 6 to 9. Coronal plane reconstruction from 3D imaging may be helpful for evaluating scoliosis and extraforaminal disease.

b. CSF flow imaging of the spine [62-65]

CSF flow can be imaged with phase-contrast cine MRI evaluation. Cardiac gating with either ECG or peripheral leads can be used to reduce cardiac-dependent flow artifacts. These approaches also permit quantitative velocity and qualitative vector measurements of CSF flow. Spinal CSF flow imaging is performed in the axial and/or sagittal planes.

Typical parameters are as follows: Cardiac gating, flip angle 20 degrees, TR/TE 20/5 ms, slice thickness 5 mm, field of view 180 mm, matrix 256 x 256, and encoding velocity (venc) 10 cm/s.

Common indications for phase contrast cine imaging in the spine include evaluation of flow dynamics at the craniocervical junction in patients with Chiari I malformation as well as craniocervical and whole spine imaging of patients with idiopathic syringomyelia in the search for myelographically occult arachnoid cysts or webs.

c. T1-FLAIR vs. FSE T1 imaging of the spine [66-69]

T1 fast spin echo (FSE) is a routine pulse sequence for imaging of the spine and can provide anatomic detail at a relatively short acquisition time compared with conventional spin echo imaging. However, T1 FSE often suffers from poor image contrast.

Fast T1-FLAIR (fluid-attenuated inversion recovery) imaging is a newer technique and takes advantage of short image acquisition with T1-weighting as well as suppression of CSF signal. While both T1 FSE and fast T1-FLAIR of the spine are useful for demonstrating normal anatomic structures and determining the presence of both degenerative and neoplastic processes of the spine, there are advantages to using fast T1-FLAIR imaging of the spine at higher magnetic field strengths. Recent evidence at 3T suggests that fast T1-FLAIR imaging allows for superior conspicuity of normal tissue interfaces as well as spinal cord lesions and abnormal vertebral body marrow. Due to the increased T1 values at higher magnetic field strength that result in reduced T1 contrast, fast T1-FLAIR has

improved CSF nulling and higher contrast-to-noise ratio (CNR), as compared to T1 FSE. Additionally, there is a reduction in susceptibility artifacts from the presence of metallic hardware using T1-FLAIR as compared to T1 FSE due to multiple 180 degree refocusing pulses; however, the echo train length (ETL) must be optimized in order to avoid the blurring artifacts at longer ETL. T1-FLAIR may also reduce specific absorption rate (SAR), which can be a limiting factor at higher fields.

d. Chemical shift imaging [70-74]

Chemical shift imaging also known as opposed phase or in-and-out of phase imaging, is a modality that is relatively new to the field of spinal MRI. The technique takes advantage of small differences in precession frequencies of lipid and water protons to determine the presence of intracellular lipid and water within the same imaging voxel. It can therefore be used to aid in distinguishing between marrow-replacing processes and marrow-preserving processes. Specifically, the technique has shown promise in the ability to distinguish pathologic from benign compression fractures, and there are data that support the ability of opposed-phase imaging to differentiate benign vertebral lesions (hemangiomas, degenerative endplate changes, etc.) from malignancy. The T1-weighted GRE sequences can be rapidly acquired, with a total scanning time of less than 5 minutes. Preliminary studies of the utility of chemical shift imaging in the spine have shown promise, and the technique is becoming more widely accepted in routine clinical practice.

e. Perfusion

MR perfusion-weighted imaging (PWI) has enjoyed great clinical and research success in assessment of cerebrovascular reserve and as an adjunct for assessing biologic behavior of cerebral neoplasms. PWI use rapid data acquisition techniques to generate temporal data series that capture the first pass kinetics of a contrast agent as it passes through a tissue matrix. PWI uses three general contrast mechanisms, (1) dynamic susceptibility contrast (DSC), which uses a gradient echo technique; (2) dynamic contrast enhancement (DCE), which uses T1-weighted methods; and (3) arterial spin labeling (ASL), which uses radiofrequency tagging of spins to elicit the contrast mechanism. Both DSC and DCE methods are based on the first pass kinetics of gadolinium contrast, whereas ASL uses unique RF tagging to generate the contrast mechanism. PWI has been less commonly used in the spine; however, several investigators have examined its potential in helping to discriminate spine lesions and to assess the vascular reserve in the spinal cord.

In the setting of neoplasia, MR-PWI is thought to provide physiologic information about the microcirculation of tumors, with the PWI metrics being a direct reflection of angiogenesis, vascular density and capillary permeability. It has also been utilized to discriminate pathologic and benign insufficiency fractures with variable success, and in conjunction with diffusion-weighted imaging (DWI), to improve the specificity in discriminating benign and malignant spine bone tumors. Chen et al used PWI to differentiate benign from metastatic compression fractures in 42 patients. They found that while metastatic lesions exhibited higher absolute peak enhancement characteristics and steeper slope than chronic compression fractures, PWI did not reliably discriminate acute benign compression fracture from malignant compression fracture [75].

Tokuda et al used DCE techniques to evaluate 48 benign and pathologic vertebral compression fractures. Enhancement characteristics were classified into five time-intensity curve subtypes. Steepest slopes were characteristic of metastatic lesions with or without pathologic fracture; however, there were insufficient features found to make this clinically useful as a decision support tool [76]. Sun et al evaluated 39 spine tumors with DWI and PWI and found that the accuracy of MR-PWI (89.7%) was greater than MR-DWI (79.5%), noting that benign vascular tumors were falsely positive on PWI. They concluded that combined PWI/DWI would lead to greater diagnostic specificity [77]. Biffar et al developed a more sophisticated methodology to assess the tissue composition of vertebral bone marrow by accounting for contributions by fat and tissue water fractions. They concluded that

correcting for the fat component in the baseline signal and parametrization by tracer-kinetic analysis are necessary to avoid diagnostic errors [78].

Small case series have used PWI to assess spinal cord vascular reserve in specific clinical applications. One case report used PWI to show alteration in spinal cord perfusion metrics in the edematous region of the spinal cord from a spinal dural arteriovenous fistula [79]. In another investigation PWI techniques were successfully used to discriminate recovery characteristics in patients with cervical spondylitis myelopathy before and after decompressive surgery. The investigators showed that reduction in mean transit times (MTT) after surgery correlated with neurologic recovery [80]. While interesting observations have been made regarding application of MR-PWI in the spine, there is no substantial class A evidence to suggest that these technique are of clinical benefit at this time.

f. Dynamic imaging/motion studies

Dynamic MR imaging of the spine is the natural extension of other types of imaging which attempt to visualize the relationships of the spinal components during physiologic loading or in varying stages of position. The most conventional form of imaging that is in common use historically is lateral flexion-extension radiography of the spine to assess for areas of segmental instability. There are known alterations in spinal canal diameter and neural foraminal size between extremes of flexion and extension. Hyperextension produces bulking of the ligamentum flavum that can produce dynamic mechanical causes of cervical spondylotic myelopathy. Prior investigations principally used myelography and postmyelographic CT, although more recently MRI has been used.

As MRI provides exceptional simultaneous soft tissue and bone detail in unlimited imaging planes, it is a logical next approach to evaluate dynamic dimensional changes to neural axis and neural elements. However, capabilities to study the spine under physiologic load are limited on most conventional scanners. Whereas flexion/extension radiography is performed in an upright position to simulate physiologic loading, conventional MRI is performed recumbent. This deficiency has led to several technical developments that in theory more closely replicate physiologic loading by incorporating gravity and thus direct axial loading to the spinal axis. This includes upright MRI and compression devices that can provide an equivalent axial load to the spinal axis even while imaging in the supine position. The latter is more limited in capability in that it does not facilitate imaging in extremes of position; rather it only replicates normal physiologic load imposed by gravity in the upright position.

Upright MRI units in particular are designed to image the spine in a variety of normal physiologic conditions: supine, upright, sitting, flexion, extension, or a combination of postures. Moreover, these devices are designed to demonstrate anatomic changes between modes of positioning. A number of investigations have been performed using flexion/extension MRI to study changes in the disc/ligament complexes and their effect on the spinal cord and neural elements.

A study by Kanno et al confirmed that axial loaded lumbar MRI will show a significant reduction in spinal canal diameter compared to a passive recumbent MRI, with a sensitivity of 96.4% and a specificity of 98.2%. Axial loaded MRI more closely replicated the findings of upright lumbar myelography [81]. This group also showed significant correlation between reduction in spinal canal cross-sectional area in axial-loaded MRI and severity of lower extremity symptoms such as walking distance, JOA score, and leg numbness. Moreover, these changes were not evident on the conventional MRI studies [82]. Alyasa et al showed increased conspicuity of annular fissures in upright extension MRI compared to conventional supine imaging [83].

In a large retrospective study using kinematic MRI in 315 patients, Kong et al demonstrated increased prevalence of instability or abnormal translational motion in patients with advanced degenerative disc disease and facet joint osteoarthritis compared to lower grades of degeneration. Ligamentum flavum hypertrophy was associated with abnormal translational and angular motion, and the combination of

interspinous ligament degeneration and paraspinal muscle denervation were associated excessive abnormal angular motion [84]. In another study, 553 patients underwent kinematic MRI to determine whether position improves diagnostic sensitivity in detecting lumbar disc herniations. Extension and flexion upright MRI revealed 16.5% and 12% more disc herniations, respectively, than those visible in neutral position [85].

Although kinematic or dynamic MRI offers some intriguing physiologic information regarding potential segmental instability, there is very little supportive evidence that this additional information correlates with individual patient symptoms or improves patient outcomes after therapy.

g. Diffusion

Diffusion imaging has been applied for imaging of vertebral body disease and spinal cord abnormalities. Reports of the performance for bone lesions have been variable, with some authors finding relatively poor sensitivity and specificity when diffusion imaging is considered in isolation, but a useful adjunct to T1 weighted imaging when used in combination [86]. Smaller diffusion coefficients in osseous metastases than normal marrow have been attributed to higher cellular density in malignant than in benign conditions. For example, Bun et al reported perfect separation of sacral insufficiency fractures from metastases by diffusion MR [87]. Similar findings have been reported, and the same mechanism invoked by other authors [88-90], but others have found no incremental contribution of diffusion to distinguishing benign from metastatic disease [91].

For spinal cord lesions, there is ample evidence, and more reason to expect, that diffusion imaging should be of similar value as in the brain. However, spinal diffusion imaging faces technical limitations not encountered when studying the head. The most challenging are motion of the spinal cord, and susceptibility artifacts that cause image distortion, particularly for echo planar approaches. Currently popular solutions revolve around reduced field of view imaging. Currently two major approaches are under active investigation. One method is to perform conventional excitation and suppress the signal from outside the desired field of view. These outer volume suppression (OVS) methods have been successfully applied in spinal cord imaging, often with fast spin-echo acquisitions to further control susceptibility artifacts [92]. Another approach is to selectively induce signal only from the desired FOV. Several authors have also used these inner volume excitation (IVE) methods; for example, the interleaved multisection inner volume (IMIV) approaches [93].

Using these methods, authors have applied diffusion-weighted spinal cord imaging to map the characteristics of normal tissue [93-94] in chronic spinal cord injury [95], cervical spontaneity myelopathy [96], intramedullary neoplasms [97], and demyelinating disease [98-99]. In all of these conditions diffusion imaging helps identify axonal loss, myelin loss, and, in the early stages of disease, axonal injury. Tractography can highlight axonal injury as seen as loss of fractional anisotropy. The usual application of tractography, to determine fiber direction, is of little significance in the spinal cord, where one knows the fiber orientation.

Although diffusion imaging is a critical component of MR evaluation of brain stroke, it has been far less studied for spinal cord ischemia. This is likely largely due to the relative rarity of spinal cord infarction. The above-mentioned conditions, especially trauma and inflammation, are far more common causes of myelopathy.

VII. DOCUMENTATION

Reporting should be in accordance with the [ACR Practice Parameter for Communication of Diagnostic Imaging Findings](#).

VIII. EQUIPMENT SPECIFICATIONS

The MRI equipment specifications and performance must meet all state and federal requirements. The requirements include, but are not limited to, specifications of maximum static magnetic strength, maximum rate of change of magnetic field strength (dB/dt), maximum radiofrequency power deposition (specific absorption rate), and maximum acoustic noise levels.

IX. QUALITY CONTROL AND IMPROVEMENT, SAFETY, INFECTION CONTROL, AND PATIENT EDUCATION

Policies and procedures related to quality, patient education, infection control, and safety should be developed and implemented in accordance with the ACR Policy on Quality Control and Improvement, Safety, Infection Control, and Patient Education appearing under the heading *Position Statement on QC & Improvement, Safety, Infection Control, and Patient Education* on the ACR web site (<http://www.acr.org/guidelines>).

Specific policies and procedures related to safety should be in place along with documentation that these policies and procedures are updated annually and that they are formulated under the supervision and direction of the supervising MRI physician. Guidelines should be provided that deal with potential hazards associated with MRI examinations to the patients as well as to others in the immediate area. Screening forms must also be provided to detect those patients who may be at risk for adverse events associated with the MRI examination.

Equipment performance monitoring should be in accordance with the ACR Technical Standard for Diagnostic Medical Physics Performance Monitoring of Magnetic Resonance Imaging (MRI) Equipment.

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